



# Stressed out: What speech tells us about stress

Will Paul<sup>1</sup>, Cecilia Ovesdotter Alm<sup>2</sup>, Reynold Bailey<sup>1</sup>, Joe Geigel<sup>1</sup>, Linwei Wang<sup>1</sup>

<sup>1</sup> Golisano College of Computing & Information Science

<sup>2</sup> College of Liberal Arts

Rochester Institute of Technology

{whp3652\*, coagla\*, rjb†, jmg†, lxwast\*}@{rit.edu\*, cs.rit.edu†}

## Abstract

Stress can have a negative and costly impact on people’s lives. Mitigating stress before it becomes a problem requires early, noninvasive identification and a deeper understanding of the signals of stress. To test automatic stress detection a new dataset was created with subjects completing the Stroop task under unstressed and stressed conditions. This paper examines to what degree speech features respond to stress and if so, what features are most informative. Features were extracted from recorded speech data and trained with several classification algorithms. We explored binary classification of stressed vs. unstressed across gender and per gender, with the best results on a held-out test set improving over the majority class baseline (MCB) by 16% across genders and with 20% and 21% for the female and male subsets respectively. Overall maximum intensity emerged as the most informative feature when comparing across classification conditions. In addition, we explored leave-one subject-out classification, resulting in a 15% improvement on average considering both genders when using random forests.

**Index Terms:** speech as cognitive marker, stress, Stroop task, stress detection

## 1. Introduction

Psychological stress has been shown to have a negative effect on cognition as well as mental and physical well-being [1, 2]. It also adversely impacts productivity in the workforce. In particular, stress has been linked with impaired problem-solving [3] and poor organizational practices [4]. Understanding the underlying signals and physiological factors that indicate whether a person is stressed is the first step towards prevention.

Existing tests for stress detection often require expensive or invasive laboratory tests such as MRI scans [5] or saliva samples [1]. Research into noninvasive approaches have primarily focused on biophysical sensors such as heart rate variability [6] or galvanic skin response [7]. Speech-focused research has mostly been evaluated within the context of automatic speech recognition (ASR) systems [8, 9], without the wellness of the end user in mind. One advantage of using speech data is that it is one of the least invasive and most natural signals to collect.

This paper explores speech data collected experimentally under unstressed and stressed conditions to determine its effectiveness for stress detection.

## 2. Related work

One of the first speech datasets focused on stress was the *Stress Under Simulated and Actual Stress* corpus [10], comprising data from 32 individuals, under different situations primarily with a closed set of words from the avionics domain. One

study found that humans have trouble classifying emotional state based on single words, achieving 58% accuracy on average over a 13% baseline [11]. A computational approach attempted to discriminate medium and high stress speech from neutral, fear, and screaming [12]. They achieved just under 75% and 60% accuracy for high and medium stress respectively over a 20% baseline. While impressive this seems skewed by the straightforward fear and screaming classes. In particular the accuracy on the screaming class approached 100%.

Another stress study examined speech data from (mostly male) helicopter pilots talking to air traffic control followed by high stress speech as they were about to crash [13]. Their analysis of pitch found that across speakers only maximum pitch and to a lesser extent mean pitch were useful. An important distinction in this study was that the stress expressed in their data was, ‘closer to terror than to task-induced anxiety.’

The search and rescue corpus for stress detection used a collaborative task to gather data from 2 subjects who work together remotely, communicating via handheld transceivers [14]. Stress was induced three-quarters of the way through by introducing a time limit and an additional task. A classifier trained on data from 8 subjects (7 males, 1 female) achieved 76% accuracy, which represented an 8% improvement over the MCB (the dataset was weighted towards the unstressed case) [15]. When tested with data from held-out subjects the algorithm performed worse, even below their MCB when averaged across subjects. They found that maximum/mean intensity and mean/median pitch to be the most important features.

## 3. Experiment design and data

A limitation of most existing speech datasets for stress detection was that they only consider spoken data [10, 13, 14]. To address this limitation the data collection experiment was structured such that other sensors could be included. We conducted this experiment in a naturalistic work environment, specifically at a stationary desk in a relatively quiet office. We used consumer grade sensor equipment, a standard lavalier microphone and recording device,<sup>1</sup> to simulate a real-world context where controlled studio recording is not possible.

Prior research has shown that it is difficult to discriminate between cognitive load and stress [16]. Thus, we selected the Stroop task [17], which is used to establish cognitive load. In this task the subject is shown a color word written in a font color different than the word itself. The subject is then tasked with saying the color of the font (e.g. if the word *black* is written in a red-colored font, the correct response is ‘red’). The Stroop task has been shown to be a challenging task for fluent speakers, be-

<sup>1</sup>Zoom H1 Handy Portable Digital Recorder.

cause different parts of the brain are involved in the processing of language and color [18].

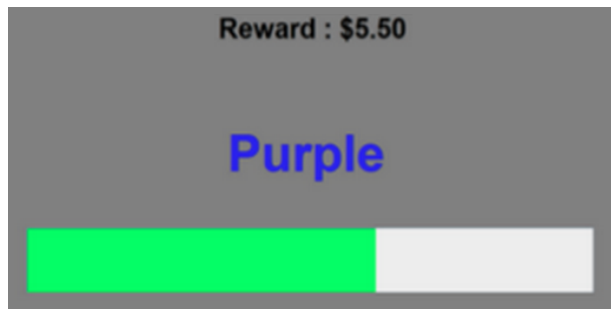


Figure 1: A screenshot of the stressed version of the Stroop task used in our data collection experiment. The unstressed version did not have the progress bar or reward counter.

Besides the regular Stroop task, we added a second, modified Stroop task, in which stressors were introduced on top of cognitive load. Accordingly, the Stroop task was conducted in two separate trials: an unstressed version where the subjects were given unlimited time to respond and a stressed version where they had 1.5 seconds to respond and for every incorrect or late answer they lost \$0.75 of their \$10 bonus (see Figure 1 for a screenshot). A practice trial was first performed to familiarize the subject with the task. There was also a rest period between the following two trials to minimize the chance that the previous trial would impact the next (see Figure 2 for an overview).

Each trial had a total of 35 lexical items and was collected from 27 subjects, for a total of 1,890 data points. The subjects were graduate and undergraduate students ages 18 to 32, comprising 16 males and 11 females with 10 of the subjects being non-native English speakers. All but three participants self-reported an increase in stress between trials, and there was a general upwards trend in the stressed trial (see Figure 3). We explored classification across gender versus by gender, resulting in three data subsets: female and male, female, and male.

## 4. Methodology

The processing of the speech data was done automatically with Praat [19]. Utterance boundaries were marked through silence detection and time-aligned with the written transcripts. As the speech data from the Stroop experiment is highly structured

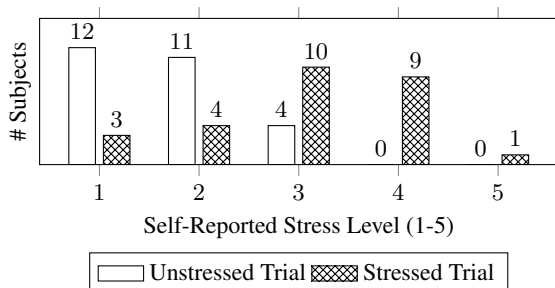


Figure 3: The post-experiment survey asked subjects to rate their stress level on a scale from 1 to 5 for each trial. This plot shows that in general, as expected, the subjects' perception of their own stress levels increased in the stressed trial.

### Pitch (Mel)

Mean, Standard Deviation, Min, Max, First Quartile, Median, Third Quartile, Mean Absolute Slope, Jitter, Normalized Time of Min (%), Normalized Time of Max (%)

### Intensity (dB)

Mean, Standard Deviation, Min, Max, First Quartile, Median, Third Quartile, Mean Absolute Slope, Shimmer, Normalized Time of Min (%), Normalized Time of Max (%)

Table 1: Features automatically extracted from the speech data with Praat [19]. Gender was considered for pitch ranges when extracting pitch information.

Female & Male	Female	Male
Min Int.	<b>Max Int.</b>	Q1 Pitch
<b>Max Int.</b>	Int. Mean Abs. Slope	Min Pitch
Med Int.	Pitch Mean Abs. Slope	Mean Pitch
Time of Min Int.	Q1 Int.	<b>Max Int.</b>
Shimmer	Q3 Int.	Min Int.

Table 2: The top five features by information gain for each subset of data. Max intensity is the only feature to occur in each.

(single words with pauses in between) automated alignment performs adequately. For each of these utterances pitch and intensity features were extracted (see Table 1 for a comprehensive list). While temporal features (e.g., response delay, utterance duration) were extracted during development and proved useful, they were not used for final classification, because the experiment included a time constraint to induce stress. The only features related to time that were included in the classification were related directly to pitch and intensity and were normalized to avoid encoding durational relationships. Syntactic and semantic features were also unavailable since the data consists of a fixed set of isolated color types; we leave this for future work. Disfluencies like repairs, fillers, and false starts were considered, but were too infrequent in the data to influence results.

Standardization of feature sets has improved speech classification in the past, in one study increasing accuracy by 11-18% [15]. For this reason standardization was implemented per person, gender, and across the whole dataset. These options were examined as an experimental parameter in a classification tuning phase. The standardization method implemented used the mean and standard deviation for each feature to convert each data point into z-scores, which indicate the number of standard deviations between an individual data point and the mean.

Feature selection was also tested as an experimental parameter during a classification tuning phase. This was done to automatically eliminate low-variance features and to compare feature importance outside of the context of a given classifier. In addition to including all features, two Scikit-learn [20] feature selection algorithms were tested: information gain from an entropy-based decision tree and a linear SVM-based approach [21]. The top five features for each data subset based on information gain are listed in Table 2.

Four machine learning algorithms were explored to model this binary classification task, including random forest, k-neighbors, decision tree, and naive Bayes, all using Scikit-learn's implementations [20]. Each data subset (female, male, and both) was split randomly into 80% train and 20% test, while

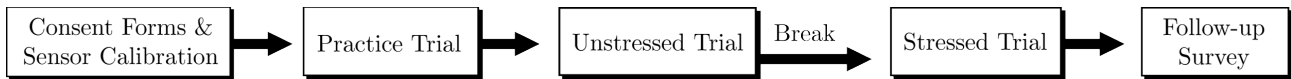


Figure 2: An overview of the procedure used for collecting data from each subject.

keeping an even 50% majority class baseline.

For each training set and each of four machine learning algorithms 10-fold cross-validation was performed, tuning the algorithms parameters and feature space. Finally, the whole training set was refit with the best combination of parameters found from the cross-validation on the training data only.

Two sets of classification experiments were completed. The first involved the data splits and tuning of parameters as described above, with model evaluation on a held-out test set. The second involved leave-one subject-out cross-validation (LOSOCV), for each fold training on k-1 subjects and leaving a distinct subject aside for evaluation. The first scenario thus addressed the problem of overfitting when considering all data instances, whereas the second analyzed performance when faced with unseen speakers, not encountered during classifier training. Because our subject count was modest and to ensure a controlled set-up, the experimental parameters from the first scenario were kept constant in the second LOSOCV approach.

## 5. Results

In the first classification scenario, the k-neighbors classifiers had more consistent performance across data subsets (see Figure 4). As expected the simple naive Bayes classifier had the worst accuracy across the board. Somewhat surprisingly the decision tree slightly outperforms the random forest classifier in two data subsets. A visualization of the decision tree for the female and male dataset is shown in Figure 6. In addition, standardizing features with z-scores slightly improved results across data subsets, regardless of the data subset used to calculate them, though in the end the best performing classifiers all used z-scores calculated across the entire data subset. Feature selection experimentation did not show consistent behavior; it varied slightly between algorithm, inclusion/exclusion, and dataset.

The best results per subset of data are as follows: k-neighbors for the whole dataset with an accuracy of 66%, k-neighbors for the male dataset with an accuracy of 71%, and random forest for the female dataset with an accuracy of 70% (see Table 4 for confusion matrices for each). All demonstrate substantial improvement over the baseline. The experimentation also illustrates the challenge of combining speech data across genders, as even after standardization the features show wide variation. See Table 5 for detailed precision and recall.

Average subject accuracy per algorithm from the LOSOCV experiment is shown in Figure 5. The random forest algorithm performed best for each data subset and maintained similar accuracy scores to the previous experiment. This suggests that it is the more robust approach for new speakers. This also shows that even though k-neighbors consistently performed well on the held-out test set, it does substantially worse on subjects it had not seen before, implying it overfits and does not generalize well to new speakers. Both the decision tree and naive Bayes classifiers experienced a less prominent drop in improvement (15% to 10% and 8% to 5% respectively on the female and male data).

Interestingly, regardless of approach the LOSOCV models

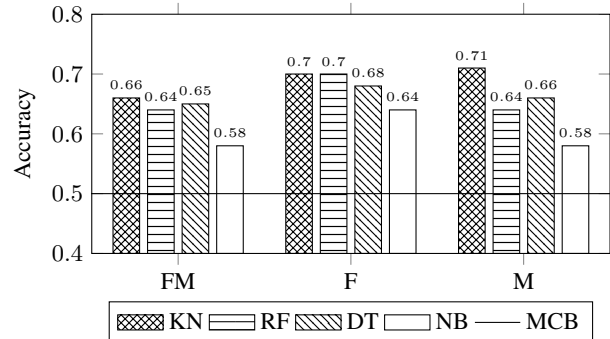


Figure 4: Accuracy on the held-out test set scenario for each algorithm's best parameters against each data subset. KN is k-neighbors, RF is random forest, DT is decision tree, and NB is naive Bayes. The baseline (MCB) is marked by a solid line. FM is female and male, F is female, and M is male.

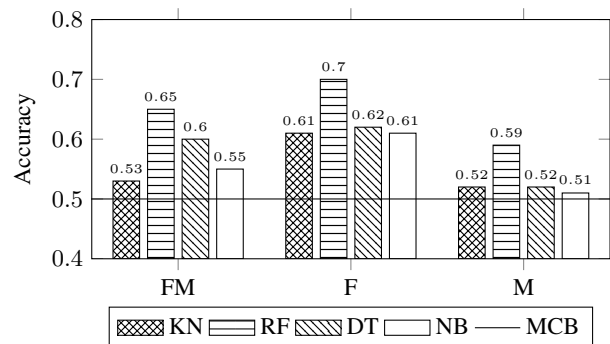


Figure 5: Mean accuracy for LOSOCV scenario. The parameters from the last experiment held constant. In this scenario, random forests performs best, even improving slightly in the per gender (M vs. F) conditions. Other algorithms, including k-neighbors, show weaker performance.

consistently excel and struggle with the same subjects. Specifically there were 5 subjects that none of the classifiers improved over the MCB and there were 5 that did so by 18% or more (see Table 3 for the 3 best and worst). Misclassification could be because the subjects were not actually stressed (see subjects E and F who did not report an increase in stress for the stressed trial), but that is not the whole story as subject D reported the largest increase of stress in the dataset, yet was classified incorrectly more than half the time. Additionally, these examples highlight that for stress inference, while speech features can be insightful for some subjects, for others they are not—pointing to the need to complement speech assessment with other multimodal features. This also might indicate that individuals react differently to stress in a way that standardization can not counteract.

A potential limitation in the dataset was that across both Stroop trials (unstressed vs. stressed) most subjects did not make any mistakes in naming the font colors. A few subjects

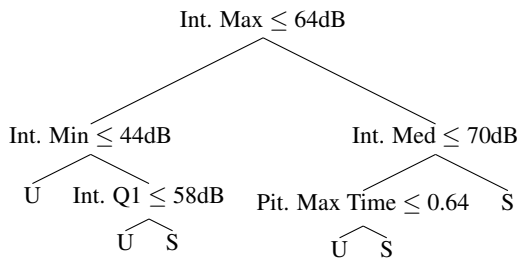


Figure 6: The decision tree created for both genders. Left nodes are accepted when the parent condition is true and right when it is false. S means the input is classified as stressed, U unstressed. This classifier achieved a 15% improvement over the MCB on the held-out test set. This points to the importance of intensity features, including maximum intensity as the root node.

Id.	Avg.	KN	RF	DT	NB	U	S
A	21%	14%	27%	19%	25%	3	4
B	25%	10%	34%	17%	37%	1	2
C	23%	9%	40%	27%	17%	2	4
D	-6%	-4%	-4%	-1%	-10%	1	4
E	-15%	1%	-20%	-20%	-20%	1	1
F	0%	6%	-9%	9%	-7%	1	1

Table 3: The 3 best (A-C) and worst (D-F) performing subjects by average accuracy improvement over MCB from the LOSOCV experiment, along with self-reported stress levels (1-5) for the unstressed trial (U), and the stressed trial (S).

mentioned that to make the task easier they let the screen go out of focus so the word became a blob of color. Another possible reason for the lack of mistakes is that 10 of the subjects were non-native English speakers, which depending on their fluency, might make the task easier as they might not internalize the words' meaning in the same way. Yet, many realistic contexts will involve non-native speakers, so their inclusion is important. Overall, it will be useful to continue to explore different methods to gather similar data. Also, in this study, the feature standardization process considered for the full data subsets; future work could explore the impact of only considering training data for that step.

	FM		F		M	
	S	U	S	U	S	U
S	123	66	56	21	76	36
U	64	125	25	52	29	83

Table 4: Confusion matrices (columns are predicted and rows are the gold standard) for the algorithm with the best performance on each held-out test set, which was k-neighbors for the female and male subset and male subset and random forest for the female subset.

## 6. Conclusion and future work

A new dataset was created and was classified with promising improvements over MCB, achieving good results even with an approach as simple as the decision tree in Figure 6. K-neighbors

	FM		F		M	
	P	R	P	R	P	R
unstressed	0.66	0.65	0.69	0.73	0.72	0.68
stressed	0.65	0.66	0.71	0.68	0.70	0.74
mean	0.66	0.66	0.70	0.70	0.71	0.71

Table 5: The precision (P) and recall (R) of the best models for each data subset, for the stressed and unstressed trials.

tended to do best on random held-out test, but failed to work well with data from previously unseen speakers in the LOSOCV experiment. The random forest classifier on the other hand maintained stable accuracy rates in both cases, showing that it is probably a more robust approach.

These results demonstrate that pitch and intensity features can be useful for predicting stress. There was some flux in the top features between the three data subsets, with one feature showing up in the top 5 of all three (maximum intensity). This limited overlap could reflect that pitch is notably variable in females (even after standardization) such that its effectiveness is limited, while for men it seems as useful as intensity measures. This matches the findings of two other studies [13, 15], whose datasets were weighted towards males.

Some spectral and formant features were useful for another stress detection research study [15] (though less important than pitch and intensity), so it may be worthwhile exploring its effect on our data. That said, another study warns that spectral features often encode too much phonetic content and end up causing the model to overfit to the content [22].

The LOSOCV experiment illustrates the challenge of speaker variability, which is in line with the results of [15]. In some cases subjects have the opposite response to the two trials. This may be due to a variable outside of stress or that the subjects are not actually stressed. This is an issue with relying on task-induced labels in general and in the future using biophysical sensors to help verify actual stress levels may help to address this. Even so, it is likely that people can respond differently to the same pressures and any detection system will need to handle this variability.

Moving forward one aspect to explore may be personalized, adaptive models that use the speaker's differences to its advantage, rather than aiming to remove them through standardization. This method has been used to some success in the biophysical and medical domain using for example personalized feature mapping [23] or continuously updating neural networks [24]. Another approach is to aggregate data from a number of multimodal sensors, the thought being that even if one modality does not work for a particular individual some other modality in the system will. Since biophysical and behavioral data was collected for this research alongside speech data both avenues are available for future work.

## 7. Acknowledgment

Thanks to the group and fellow researchers Brendan John, Vasudev Bethamcherla, Taylor Kilroy, and Krithika Sairamesh.

This work was supported by a Golisano College of Computing and Information Sciences Kodak Endowed Chair Fund Health Information Technology Strategic Initiative Grant.

## 8. References

- [1] J. Yang, M. Qi, L. Guan, Y. Hou, and Y. Yang, "The time course of psychological stress as revealed by event-related potentials," *Neuroscience Letters*, vol. 530, no. 1, pp. 1–6, 2012.
- [2] H. J. Eysenck, R. Grossarth-Maticek, and B. Everitt, "Personality, stress, smoking, and genetic predisposition as synergistic risk factors for cancer and coronary heart disease," *Integrative Physiological and Behavioral Science*, vol. 26, no. 4, pp. 309–322, 1991.
- [3] E. L. Cowen, "The influence of varying degrees of psychological stress on problem-solving rigidity," *Journal of Abnormal and Social Psychology*, vol. 47, no. 2, pp. 512–519, 1952.
- [4] B. H. Jacobson, S. G. Aldana, R. Z. Goetzl, K. Vardell, T. B. Adams, and R. J. Pietras, "The relationship between perceived stress and self-reported illness-related absenteeism," *American Journal of Health Promotion*, vol. 11, no. 1, pp. 54–61, 1996.
- [5] J. Wang, H. Rao, G. S. Wetmore, P. M. Furlan, M. Korczykowski, D. F. Dinges, and J. A. Detre, "Perfusion functional MRI reveals cerebral blood flow pattern under psychological stress," *Proceedings of the National Academy of Sciences of the United States of America*, vol. 102, no. 49, pp. 17 804–17 809, 2005.
- [6] P. Karthikeyan, M. Murugappan, and S. Yaacob, "Analysis of Stroop color word test-based human stress detection using electrocardiography and heart rate variability signals," *Arabian Journal for Science and Engineering*, vol. 39, no. 3, pp. 1835–1847, 2014.
- [7] J. Bakker, M. Pechenizkiy, and N. Sidorova, "What's your current stress level? Detection of stress patterns from GSR sensor data," in *2011 IEEE 11th International Conference on Data Mining Workshops (ICDMW)*. IEEE, 2011, pp. 573–580.
- [8] J. H. Hansen, "Analysis and compensation of speech under stress and noise for environmental robustness in speech recognition," *Speech communication*, vol. 20, no. 1, pp. 151–173, 1996.
- [9] J. H. Hansen and S. Patil, "Speech under stress: Analysis, modeling and recognition," in *Speaker Classification I*. Springer, 2007, pp. 108–137.
- [10] J. H. Hansen, S. E. Bou-Ghazale, R. Sarikaya, and B. Pellom, "Getting started with SUSAS: A speech under simulated and actual stress database," in *Proceedings of EUROSPEECH*, vol. 97, 1997, pp. 1743–46.
- [11] R. S. Bolia and R. E. Slyh, "Perception of stress and speaking style for selected elements of the SUSAS database," *Speech Communication*, vol. 40, no. 4, pp. 493–501, 2003.
- [12] B. Vlasenko, B. Schuller, A. Wendemuth, and G. Rigoll, "Combining frame and turn-level information for robust recognition of emotions within speech," in *Proceedings of INTERSPEECH*, 2007, pp. 2249–2252.
- [13] A. Protopapas and P. Lieberman, "Fundamental frequency of phonation and perceived emotional stress," *The Journal of the Acoustical Society of America*, vol. 101, pp. 2267–2277, 1997.
- [14] K. Eberhard, H. Nicholson, S. Kübler, S. Gundersen, and M. Scheutz, "The Indiana "cooperative remote search task" (CReST) corpus," in *Proceedings of the Seventh conference on International Language Resources and Evaluation (LREC'10)*. European Languages Resources Association (ELRA), 2010. [Online]. Available: <http://aclweb.org/anthology/L10-1459>
- [15] M. Frampton, S. Sripada, R. A. H. Bion, and S. Peters, "Detection of time-pressure induced stress in speech via acoustic indicators," in *Proceedings of the 11th Annual Meeting of the Special Interest Group on Discourse and Dialogue*. Association for Computational Linguistics, 2010, pp. 253–256.
- [16] C. Setz, B. Arnrich, J. Schumm, R. La Marca, G. Troster, and U. Ehlert, "Discriminating stress from cognitive load using a wearable EDA device," *IEEE Transactions on Information Technology in Biomedicine*, vol. 14, no. 2, pp. 410–417, 2010.
- [17] J. R. Stroop, "Studies of interference in serial verbal reactions," *Journal of Experimental Psychology: General*, vol. 121, no. 1, p. 15, 1992.
- [18] C. M. MacLeod, "Half a century of research on the Stroop effect: an integrative review," *Psychological bulletin*, vol. 109, no. 2, p. 163, 1991.
- [19] P. Boersma and D. Weenink, "Praat: Doing phonetics by computer (version 5.1.13)," 2009. [Online]. Available: <http://www.praat.org>
- [20] F. Pedregosa, G. Varoquaux, A. Gramfort, V. Michel, B. Thirion, O. Grisel, M. Blondel, P. Prettenhofer, R. Weiss, V. Dubourg, J. Vanderplas, A. Passos, D. Cournapeau, M. Brucher, M. Perrot, and E. Duchesnay, "Scikit-learn: Machine learning in Python," *Journal of Machine Learning Research*, vol. 12, pp. 2825–2830, 2011.
- [21] J. Brank, M. Grobelnik, N. Milic-Frayling, and D. Mladenic, "Feature selection using linear support vector machines," in *Proceedings of the 3rd International Conference on Data Mining Methods and Databases for Engineering*, 2002.
- [22] B. Schuller, G. Rigoll, and M. Lang, "Hidden Markov model-based speech emotion recognition," in *Proceedings of 2003 IEEE International Conference on Acoustics, Speech, and Signal Processing*, vol. 2. IEEE, 2003, pp. II–1.
- [23] Y. Shi, M. H. Nguyen, P. Blitz, B. French, S. Fisk, F. De la Torre, A. Smailagic, D. P. Siewiorek, M. alAbsi, E. Ertin *et al.*, "Personalized stress detection from physiological measurements," in *International Symposium on Quality of Life Technology*, 2010, pp. 28–29.
- [24] W. Jiang and S. G. Kong, "Block-based neural networks for personalized ECG signal classification," *IEEE Transactions on Neural Networks*, vol. 18, no. 6, pp. 1750–1761, 2007.